A new lipid anchor for sparsely-tethered bilayer lipid membranes

Frank Heinrich,^{1,2} Tiffany Ng,³ David J. Vanderah,⁴ Prabhanshu Shekhar,² Mihaela Mihailescu,^{1,5} Hirsh Nanda,¹ Mathias Lösche^{1,2,*}

¹Center for Neutron Research, National Institute of Standards and Technology, Gaithersburg, MD 20899-6102

²Physics Department, Carnegie Mellon University, Pittsburgh, PA 15213-3890

³Dept. of Biomedical Engineering, Johns Hopkins University, Baltimore, MD 21218

⁴Chemical Sciences and Technology Laboratory, National Institute of Standards and Technology, Gaithersburg, MD 20899-8313

⁵Department of Physiology and Biophysics, School of Medicine, University of California at Irvine, Irvine, CA 92697

*Correspondence:

Mathias Lösche,
Physics Dept., Carnegie Mellon University, 5000 Forbes Ave., Pittsburgh, PA 15213-3890
412-268-2735, fax: 412-268-8252, emb: quench@cmu.edu

ABSTRACT

Mixed self-assembled monolayers (SAMs) of β -mercaptoethanol and the new synthetic lipid 1,2-di-*O*-palmityl-3- $[\omega$ -mercapto-nona(ethylene oxide) glycerol], FC16, were investigated for their ability to form sparsely-tethered bilayer lipid membranes (stBLMs) completed with various phospholipids. We investigated the structural and functional properties of FC16-based stBLMs and compared these to stBLMs prepared using a previously characterized synthetic lipid, 1,2-di-*O*-myristyl-3- $[\omega$ -mercaptohexa(ethylene oxide) glycerol] (WC14). FC16-based stBLMs show increased resistivity to ion transfer and an increase in the submembrane space of ≈ 0.5 nm. Importantly, FC16-based stBLMs formed well-defined, complete bilayers with charged phospholipids such as POPG. In these, POPG, incorporates into the outer monolayer leaflet in the same ratio as in the immersion solution, but is excluded from the inner leaflet. In all cases we investigated thus far, the area densities of the lipids within the bilayers were on average close to those in free bilayer membranes. For charged phospholipids, FC16 appears to provide a distinct advantage over WC14 for the formation of well-defined stBLMs.

I. INTRODUCTION

Protein crystallography has revolutionized our understanding of molecular biology and is the technique of choice for determining protein structures with full atomic detail. Nevertheless, many relevant functional biological entities are in the form of disordered structures that require other techniques, such as nuclear magnetic resonance (NMR) or neutron reflectometry (NR) for their investigation. A particularly important example of a biologically active, disordered structure is the lipid bilayer membrane, a double layer leaflet of fluid lipids that provide the context for function of membrane proteins which reside in them.^{1,2} Although the lipid bilayer is in-plane disordered and merely ≈ 5 nm thin, it is highly insulating against ion transport across the membrane, which is key to many vital biological functions, from charge separation in photosynthesis to signal conduction along neuronal axons.

In order to investigate the physical properties of lipid bilayers on the molecular scale, model membranes have been employed for decades. Starting with work by McConnell's group^{3,4} bilayer models supported by solid substrates have been investigated as membrane mimics. We and others⁵⁻¹⁰ have more recently developed tethered bilayer membrane (tBLM) systems on solid support that are separated from the inorganic surface by an ultrathin hydration layer. tBLMs take advantage of a planar geometry brought about by the solid support to study molecular interactions of proteins with lipid bilayers in a system that is resilient and in-plane fluid. Typically, a synthetic lipid anchor, which tethers one or more hydrophobic chains via a hydrophilic spacer such as an oligo(ethylene oxide), is chemisorbed to the substrate surface.

Cornell and coworkers developed a tBLM system with incorporated synthetic gramicidin derivatives that modulated ion flux across the membrane by biospecific binding of analytes, thus converting chemical into electric signals.⁵ In their seminal work, they developed a technique for bilayer completion which bypassed the frequently used vesicle fusion approach with a process termed "rapid solvent exchange". In this process, a self-assembled monolayer (SAM)

of the tether lipid is incubated with an organic solution of lipids, followed by rapid replacement of the organic phase by aqueous buffer. This procedure precipitates a bimolecular layer onto the SAM that mimics well most aspects of a lipid membrane. As has been shown with NR,¹⁰⁻¹³ rapid solvent exchange intercalates lipids between the tethers in the monolayer proximal to the substrate and complements this proximal layer with a distal monolayer of lipid, thus rendering the surface hydrophilic. Phospholipids reside in this bilayer in a lateral density similar to that of lipids in free-standing bilayers, such as vesicle. Importantly, such tBLMs show usually higher electric resistance^{10,14} and lower defect density¹⁰ than bilayers prepared by vesicle fusion. NR shows also unambiguously that a thin (≈ 1 nm), stable hydration layer separates the proximal lipid monolayer from the solid substrate. Such a layer is deemed important for rendering the bilayer in-plane fluid and providing space for the insertion of transmembrane proteins into the synthetic bilayer model.

In earlier work with a specific anchor lipid, di-*O*-myristyl- ω -mercapto-hexa(ethylene oxide) glycerol (WC14), we optimized such a bilayer architecture formed on molecularly smooth Au films by recognizing that it is essential to laterally dilute the grafting points with a short hydrophilic “backfiller”,¹⁴ such as β -mercaptoethanol (β ME). We refer to the resulting membrane mimics as sparsely-tethered bilayer lipid membranes (stBLMs).

The resilience of the tBLM system may be demonstrated in various ways. For tBLMs completed with diphytanoylphosphatidylcholine, which forms particularly dense, yet fluid bilayers, Köper and coworkers showed that such membranes withstand electric d.c. fields up to several 10^8 V/cm.¹⁵ Remarkably, electrical parameters of such bilayers were shown to be stable for months.¹⁵

For characterization with NR, we routinely take advantage of this resilience by performing a multitude of measurement scans on one physical sample under multiple solvent contrasts and/or to compare the as-prepared tBLM structure with its structure under the influence of a ligand, such as a protein. For example, we have recently incorporated a bacterial toxin, α -hemolysin (α HL), in extremely high density into the tBLM and characterized the structure of the resulting protein-reconstituted membrane.¹³ Not only does the bilayer withstand various

solvent exchanges between consecutive measurements but it is also stable if perforated by a lysogenic protein such as α HL at a density of $> 10^3/\mu\text{m}^2$. Because all sample manipulations are performed *in situ* on the sample cell of the neutron instrument, consecutive NR measurements are taken on identical footprints of the neutron beam on the sample. NR emerges therefore as a prime tool for the determination of intrinsically disordered structures, such as an in-plane fluid bilayer, at a (one-dimensional) resolution that approaches 1 Å.¹³ Reflectivity measurements of polarized neutrons reflected from substrates that carry magnetic nanolayers buried underneath the gold film have been recently shown to achieve even higher resolution on extremely thin organic films.¹⁶

tBLM systems offer application potential in a broad range of biomedical investigations where the interaction of proteins with membranes is of immediate interest, such as studies into toxicology,^{13,17} Alzheimer's disease,¹² cell signaling involving lipids,¹⁸ or laminopathies.¹⁹ In this work, we describe a new lipid anchor, FC16 [1,2-di-*O*-palmityl-3-(ω -mercapto-nona(ethylene oxide) glycerol)], that we developed on the basis of WC14, in its molecular architecture and aim at its molecular characterization to form stBLMs.

II. EXPERIMENTAL SECTION²⁰

Synthesis of FC16. Preparation of FC16 (IUPAC: 29-hexadecyloxy-3,6,9,12,15,18,21,24,27,31-decaoxaheptatetracontan-1-thiol) initiated with the tetrahydropyranyl ether of 4,7,10,13,16,19-hexaoxaheneicosan-2,21-diol, **1**, (Scheme 1) available as an intermediate in the previously described synthesis of WC14,¹⁰ and proceeded through alkylation of the vicinal 1,2-dihydroxy groups, deprotection, ethylene oxide chain extension via a Williamson ether synthesis using the tetrahydropyranyl ether of the commercially available 2-[2-(2-chloroethoxy)ethoxy]ethanol, deprotection, and conversion of the newly generated, terminal hydroxyl group to the thiol as described previously.²¹

Synthesis. Tetrahydrofuran (THF) (Mallinckrodt AR) and 2-[2-(2-chloroethoxy)ethoxy]ethanol were purchased from North Strong Scientific (Phillipsburg, NJ) and TCI (Portland, OR), respectively. THF was distilled from CaH_2 immediately before use. All other chemicals were

purchased from Aldrich Chemical Co., (Milwaukee, WI) and used as received. All compounds were purified by chromatography [silica gel, J.T. Baker (Phillipsburg, NJ), 40 μ m, column = 33 cm x 3 cm]. Proton (^1H) nuclear magnetic resonance (NMR) spectra were obtained on a JOEL 270 MHz spectrometer in CDCl_3 containing 0.03% tetramethylsilane (TMS). Chemical shifts (δ) are in parts per million (PPM) relative to TMS and coupling constants (J) in Hertz (Hz). All reactions were carried out under nitrogen.

Tetrahydropyranyl ether of 20-hexadecyloxy-3,6,9,12,15,18,22-heptaooxaotatricontan-1-ol, 2-THP. To 0.192 g (8.0 mmol) NaH in 3 mL THF was added 1.11 g (2.51 mol) 1 in 5 mL THF at room temperature. After the completion of the addition, the temperature was increased to 42°C and 2.67 g (8.7 mmol) 1-bromohexadecane in 8 mL THF was added dropwise. After 3 d at 42°C the mixture was filtered, adsorbed to 7 g silica gel and chromatographed (100% ethyl acetate) to give 0.615 g of 2-THP. ^1H NMR; δ 4.63 (1 H, br. t, J = 3.0, tetrahydropyranyl OCHO methine), 0.88 (6H, br. t, J = 6, 2 $\text{CH}_3\text{C}_{15}\text{H}_{30}\text{O}$). Chromatography also afforded 0.186 g of a more polar monoalkylated product, most likely, 3,6,9,12,15,18,22-heptaooxaotatricontane-1,20-diol. ^1H NMR; δ 4.63 (1H, br. t, J = 3.0, tetrahydropyranyl OCHO methine), 0.88 (3H, br. t, J = 6, $\text{CH}_3\text{C}_{15}\text{H}_{30}\text{O}$).

20-hexadecyloxy-3,6,9,12,15,18,22-heptaooxaotatricontan-1-ol, 2: A solution of 1.05 g (1.2 mmol) 2-THP in 28 mL glacial acetic acid/THF/water (4/2/1) was maintained at 50°C for 7 h. Removal of solvents and chromatography (5% methanol/ethyl acetate) afforded 0.644 g (68%) 2. ^1H NMR; δ 3.9 to 3.4 (33 H, m, $-\text{CH}_2\text{CH}_2\text{O}-$ and $-\text{CHO}-$ protons, 2.6 (0.8 H, br. t, ROH), 1.55 (4H, br. pentet, J $\approx$ 6, 2 $\text{C}_{14}\text{H}_{27}\text{CH}_2\text{CH}_2\text{O}-$), 1.25 (52 H, br. s, 2 $\text{C}_{14}\text{H}_{27}\text{CH}_2\text{CH}_2\text{O}-$), 0.88 (6 H, br. t, J $\approx$ 6, 2 $\text{CH}_3\text{C}_{15}\text{H}_{30}\text{O}$).

Tetrahydropyranyl ether of 29-hexadecyloxy-3,6,9,12,15,18,21,24,27,31-decaoxaheptatetcontan-1-ol, 3-THP. To 0.11 g (4.6 mmol) NaH in 3 mL THF was added 0.644 g (0.8 mmol) 2 at 0°C. After the completion of the addition, the temperature was increased to 43°C. To this was added 1.09 g (4.3 mmol) $\text{Cl}(\text{CH}_2\text{CH}_2\text{O})_3\text{THP}$ in 6 mL THF and maintained at 43°C for 5 d. Water (50 mL) was added, cautiously at first, and the THF removed under reduced pressure.

The aqueous layer was continuously extracted with ethyl acetate overnight. Chromatography of the ethyl acetate residue (5% methanol/ethyl acetate) yielded 0.585 g (78%) 3-THP. ^1H NMR; δ 4.63 (1 H, br. t, $J \approx 3.0$, tetrahydropyranyl OCHO methine), 3.9 to 3.4 (47 H, $\text{CH}_2\text{CH}_2\text{O}$ - and CHO-protons), 0.88 (6H, br. t, $J \approx 6$, 2 $\text{CH}_3\text{C}_{15}\text{H}_{30}\text{O}$).

29-hexadecyloxy-3,6,9,12,15,18,21,24,27,31-decaoxaheptatetracontan-1-ol, 3. A solution of 0.585 g (0.57 mmol) 3-THP in 28 mL glacial acetic acid/THF/water (4/2/1) was maintained at 50°C for 8 h. Removal of solvents and chromatography (10% methanol/ethyl acetate) afforded 0.466 g (78%) 3. ^1H NMR; δ 3.9 to 3.4 (45 H, m, $-\text{CH}_2\text{CH}_2\text{O}$ - and $-\text{CHO}$ - protons), 2.6 (0.8 H, br. t, ROH), 1.55 (4H, br. pentet, $J \approx 6$, 2 $\text{C}_{14}\text{H}_{27}\text{CH}_2\text{CH}_2\text{O}$ -), 1.25 (52 H, br. s, 2 $\text{C}_{14}\text{H}_{27}\text{CH}_2\text{CH}_2\text{O}$ -), 0.88 (6 H, br. t, $J \approx 6$, 2 $\text{CH}_3\text{C}_{15}\text{H}_{30}\text{O}$).

30-bromo-1,2-dihexadecyloxy-4,7,10,13,16,19,22,25,28-tricontane, 4. To a solution of 0.466 g (0.50 mmol) 3 and 0.1572 g (0.60 mmol) triphenylphosphine in 7 mL dry CH_2Cl_2 was added 0.1067 g (0.6 mmol) N-bromosuccinimide in small portions then stirred overnight at room temperature. Chromatography (5% methanol/ethyl acetate) gave 0.377 g (76%) of 4. ^1H NMR; δ 3.81 (2H, t, $J = 6.5$, BrCH_2CH_2), 0.88 (6 H, br. t, $J \approx 6$, 2 $\text{CH}_3\text{C}_{15}\text{H}_{30}\text{O}$).

29-hexadecyloxy-3,6,9,12,15,18,21,24,27,31-decaoxaheptatetracontan-1-thioacetyl, 5. To 3 mL CH_3OH was added 0.0014 g (0.62 mmol) Na° . After H_2 evolution ceased, 1.06 g (1.4 mmol) CH_3COSH added followed by 0.377 g (0.377 mmol) of 4 in 5 mL CH_3OH , then refluxed for 7 h. Chromatography (5% methanol/ethyl acetate) yielded 0.351 g (94%) of 5 FC16-thiol acetate. ^1H NMR; δ 3.09 (2 H, t, $J = 6.4$, $\text{CH}_3\text{COSCH}_2\text{CH}_2$), 2.34 (3 H, s, CH_3COS), 0.88 (6 H, br. t, $J \approx 6$, 2 $\text{CH}_3\text{C}_{15}\text{H}_{30}\text{O}$).

29-hexadecyloxy-3,6,9,12,15,18,21,24,27,31-decaoxaheptatetracontan-1-thiol, FC16. A solution of 0.351 g (0.35 mmol) of 5 was refluxed for 8 h in 30 mL 0.1N HCl/ CH_3OH . Chromatography (3% methanol/ethyl acetate) afforded 0.308 g (92%) pure FC16 (m.p. 33-35°C). ^1H NMR; δ 3.7 to 3.4 (43 H, m, $-\text{CH}_2\text{CH}_2\text{O}$ - and CHO- protons), 2.70 (2H, dt, $J \approx 6.5$ and 6.2, $\text{HSCH}_2\text{CH}_2\text{O}$), 1.62 to 1.50 (5H, HS and 2 $\text{C}_{14}\text{H}_{27}\text{CH}_2\text{CH}_2\text{O}$ -), 1.25 (52 H, br. s, 2

$\text{C}_{14}\text{H}_{27}\text{CH}_2\text{CH}_2\text{O}-$), 0.88 (6 H, br. t, $J \approx 6$, 2 $\text{CH}_3\text{C}_{15}\text{H}_{30}\text{O}$). High resolution MS (ESI): $m/z = 953.7621$ (MH^+); calc. for $\text{C}_{53}\text{H}_{109}\text{O}_{11}\text{S}$: 953.7694.

Sample Preparation. 3" diameter silicon wafers (100) from Silicon Quest Intl. Inc. (Santa Clara, CA) were coated with Cr (≈ 20 Å) and Au films (≈ 150 Å for neutron reflection and ≈ 500 Å for all other measurements) by high-energy magnetron sputtering (ATC Orion, AJA Intl., Inc., North Scituate, MA). Similar to earlier work with the related compound, WC14, we prepared self-assembled monolayers (SAMs) by immersing freshly prepared Au film surfaces in 0.2 mmol/L ethanolic solutions of either FC16 or mixtures of FC16 and β -mercaptoethanol (β ME; Sigma-Aldrich, St. Louis, MO) at different mol% ratios as specified, henceforward designated, for example, as FC16: β ME = 30:70. β ME was distilled before use. After incubation, SAMs were rinsed with absolute ethanol and dried with nitrogen. Tethered lipid bilayer membranes (tBLMs) were formed by rapid solvent exchange as described.¹⁰ Phospholipids used for the completion were 1,2-phytanoyl-*sn*-glycero-3-phosphocholine (DPhyPC), 1-palmitoyl-2-oleoyl-*sn*-glycero-3-phosphocholine (POPC), 1-palmitoyl-2-oleoyl-*sn*-glycero-3-phosphoglycerol (POPG or *h*-POPG) and 1-perdeuteriopalmityl-2-oleoyl-*sn*-glycero-3-phosphoglycerol (*d*-POPG), all from Avanti Polar Lipids (Alabaster, AL) and used as supplied. Bilayers formed on mixed FC16/ β ME SAMs are henceforward referred to as sparsely-tethered bilayer membranes (stBLMs), because β ME dilutes the tether packing density at the Au surface, indicated, for example, by a more facile reconstitution of proteins into the finished bilayers, as shown in previous work.¹³

Characterization Methods. Spectroscopic ellipsometry, Fourier transform infrared reflection-absorption spectroscopy (FT-IRRAS), contact angle measurements and electrochemical impedance spectroscopy (EIS) were all performed at room temperature as previously described.^{13,21} In brief, multiple wavelength ellipsometric measurements were performed on a J. A. Woollam Co., Inc. (Lincoln, NE) M-44 spectroscopic ellipsometer aligned at a nominal incidence angle of $\approx 70^\circ$ from the surface normal.²²

p-polarized FT-IRRAS data were obtained using a Nicolet Magna-IR model 570 Series II spectrometer (Thermo Nicolet, Madison, WI) with a model FT-85 (85° grazing angle with inte-

grated polarizer) Spectra-Tech external reflection accessory (Thermo Spectra-Tech, Shelton CT). The spectrometer utilized a KBr beamsplitter and mercury cadmium telluride (MCT/A) detector. Spectra were acquired at 4 cm^{-1} resolution between 4000 and 700 cm^{-1} as a summation of 1000 scans using Happ-Genzel apodization without zero filling. Background spectra (R_0) were taken using $(\text{CD}_3(\text{CD}_2)_{17}\text{S})_2$ SAMs on Au. The sample spectra (R) were acquired under identical equipment conditions and normalized by the background spectra to obtain spectra of $-\log(R/R_0)$ vs. wavenumber.

Sessile contact angles (θ) were determined with a Ramé-Hart model 110-00-115 goniometer at ambient relative humidity using water as the probing liquid. At least four measurements were taken for each SAM by lowering a $2\text{--}3\text{ }\mu\text{L}$ drop onto the surface from a blunt-ended needle attached to a 2 mL syringe. The contact angle was recorded immediately after the drop detached from the needle tip.

EIS data were taken using a Solartron (Farnborough, U.K.) system (model 1287A potentiostat and model 1260 frequency response analyzer) and fitted to equivalent circuit models (ECMs) using *ZView* (Scribner Associates, Southern Pines, NC). Au-coated silicon wafers ($20\times 40\text{ mm}$) served as the working electrode in a setup that allowed simultaneous EIS measurements in 6 distinct electrochemical cells (volume, $V \approx 250 - 300\text{ }\mu\text{L}$) on each wafer, with their surface areas ($A_{el} \approx 0.33\text{ cm}^2$) on the Au film confined by Viton O-rings. Copper contrast was used to measure the geometric electrode surface area.²³ EIS data were normalized to A_{el} and the roughness factor β , estimated from the Au surface oxidation/oxide stripping charge.²⁴ A saturated silver-silver chloride ($\text{AgI/AgCl/NaCl(aq,sat)}$) microelectrode (Microelectrodes, Bedford, NH, model M-401F) was used as reference. The auxiliary electrode was a 0.25 mm diameter Pt wire (99.99% purity, Aldrich) coiled around the barrel of the reference electrode. The distance between the tip of the reference and working Au electrode surface was set to $2 - 3\text{ mm}$. Measurements were carried out with 10 mV a.c. at 0 V bias vs. the reference electrode in aerated solutions.

Neutron reflection data acquisition and analysis. Neutron reflectometry (NR) has been extensively used to characterize molecularly organized surfactant and lipid layers at the sub-nano-

meter level.^{25,26} NR measurements were performed on the Advanced Neutron Diffractometer/ Reflectometer (AND/R)²⁷ at the NIST Center for Neutron Research (NCNR). The resilience of the stBLMs permitted the NR characterization of the membrane at various solvent contrasts with the same physical sample. For contrast variation, solvent exchange was performed *in situ* on the instrument, so that the neutron spectra were taken on exactly the same footprints on the wafers. This insured that the inorganic substrates, in particular the SiO_x/Cr/Au surface layers that dominate the interference patterns in the data, contributed identically to subsequent measurements.

NR data analysis was performed using the optimization tool *ga_refl*,²⁸ developed at the NCNR. *ga_refl* supports the constrained fitting of multiple data sets in terms of slab models. Reflectivity is computed using an optical matrix.²⁹ *ga_refl* implements a genetic algorithm to perform a rapid search across parameter space with robustness against trapping in local minima. This genetic algorithm is used in alternation with a simplex *amoeba* algorithm.³⁰ The thus-obtained, pre-selected population of model parameters is further optimized using a Levenberg-Marquardt nonlinear least-square fit. *ga_refl* supports the simultaneous fit of a set of reflectivity curves with shared parameters between the individual reflectivity curves. In general, all reflectivity curves measured on one and the same wafer in the course of a complex experiment are fitted simultaneously sharing fit parameters, for example, for the substrate.

Data sets of isomorphic samples with distinct isotopic contrast were simultaneously fitted by refining the corresponding neutron scattering length density (nSLD) profiles $\rho_n(z)$ consistently to each other in terms of the underlying molecular structures.^{26,31} The model contains the following sequence of layers along the direction, $\hat{z}$, of the surface normal: (semi-infinite) Si wafer, SiO_x, Cr, Au, the hydrated nona(ethylene oxide) spacer, the inner leaflet and the outer leaflet of the bilayer, the outer headgroup layer, and bulk solvent. The model allows all organic layers to comprise solvent which contributes to the average scattering power of each layer according to the nSLD of the bulk solvent multiplied by its volume fraction in the layer (which may be zero in the hydrophobic core of a defect-free stBLM). Both lipid leaflets in the stBLM model were constrained to the same hydrophobic thickness because they are highly corre-

lated. These two layers can, however, contain different amounts of water that may form solvent-filled defect pockets. The inner headgroup layer of the lipid membrane was indistinguishable from the NEO tether at any solvent contrast, and was therefore not separately modeled.

Parameter confidence analysis. A Monte Carlo (MC) resampling technique³⁰ was applied to determine fit parameter confidence intervals and parameter correlations. In this approach, a large number N (typically, $N = 1000$) statistically independent sets of synthetic reflectivity data were created based on the actual experimental data and their individual error bars, *i.e.* each synthetic reflectivity curve differed in each data point from the experimental reflectivity by a random normal deviate in which the width of the applied normal distributions is given by the uncertainty σ of the measured data point based on counting statistics. Each of the synthetic reflectivity data sets is simultaneously fitted using the algorithms described above, thus producing one set of fit parameters and corresponding nSLD profile that deviate slightly from the “true” results but could have occurred given the experimental error bars associated with the actual measurement. A statistical analysis of all resampled sets of fit parameters allows the determination of confidence intervals, by measuring standard deviations of the parameter distributions, and of correlations between fit parameters. To assess parameter correlations, the covariance for any given pair of fit parameter sets a and b are calculated as

$$C_{ab} = \frac{1}{N-1} \frac{\sum_{i=1}^N (a_i - \mu_a)(b_i - \mu_b)}{\sigma_a \sigma_b} \quad (1)$$

where a_i and b_i are the i^{th} result of the ordered set of fit parameter results. $\mu_{a,b}$ and $\sigma_{a,b}$ are the arithmetic means and the standard deviations of sets a and b , respectively.

Parameters for each subsequent MC run can be initialized by either using the results of the previous iteration or using new random values. Seeding each fit with a new random set increases significantly the time required for searching parameter space, but is a powerful means of assessing whether the obtained nSLD profile corresponds to the global minimum within a chosen model. In this work, MC iterations were seeded with random values.

In addition to determining objective measures for parameter confidence, MC output also provides a convenient tool for visualizing the variational bandwidth associated with the nSLD profile due to data scatter. By mapping each nSLD profile generated in the MC resampling onto a p_n - z grid with a constant bin size, a 2D matrix is generated whose element values contain the frequency by which this element is occupied by any of the nSLD curves. This matrix may then be used to visualize $p_n(z)$ and the associated probabilities of deviations from the best-fit profile. Such plots are handy tools to determine which regions in the nSLD profiles are well defined – and which are not.

All capabilities described above have been implemented in a wrapper script in the most recent version of *ga_refl*.²⁸

III. RESULTS

Self-assembled monolayers. Mixed SAM formation was investigated over a range of FC16: β ME ratios from 100:0 to 10:90 and over a range of immersion times from 4 hours to 3 days. While it is anticipated that the larger FC16 may exhibit a slightly larger propensity to adsorb to the Au relative to β ME we do not expect that the surface-bound concentrations χ_{FC16} and $\chi_{\beta\text{ME}}$, respectively, to be substantially different from the solution concentration. Therefore, FC16: β ME ratios throughout this paper are quoted as concentrations in the adsorption solution.

While the SAMs formed quickly from solution to a completion of $\approx 90\%$ (within approx. 1 min for WC14, ref. 10), full coverage of the surface require longer immersion times. We assessed surface properties in terms of static contact angles (θ) and spectroscopic ellipsometric thickness d_{SE} estimates of the surface films after 4 h, 1 d and 3 d of immersion (Fig. 1 and Table 1). Consistently, the FC16: β ME SAMs showed high contact angles and constant organic thicknesses from 100% FC16 up to β ME molar ratios of 50%. Upon increasing the β ME concentration further, d_{SE} decayed linearly to the value for pure β ME, whereas θ decreased from $> 105^\circ$ to a plateau near 80° which persisted to β ME molar ratios of 90%, significantly larger than the low hydrophobicity of an interface modified by pure β ME ($\theta_{\beta\text{ME}} \approx 30^\circ$).

Figure 1 illustrates the behavior of d_{SE} and compares the FC14/ β ME results with those obtained for WC14: β ME in earlier work.¹⁰ Consistent with expectations based on the structural differences of FC16 and WC14, FC16/ β ME SAMs show larger thicknesses throughout the entire range of backfiller concentrations. As expected, these differences are more pronounced at high concentrations of the membrane anchors. Importantly, the regime of FC16 concentrations at which we observed the full thickness of the organic layer, $d_{SE} \approx 40$ Å, extends down to 50 mol%, significantly more than that observed with WC14: β ME = 80:20. This indicates that the longer alkyl chain increases the molecular order through enhanced van der Waals interactions. The differences in d_{SE} at high lipid anchor concentrations (≈ 40 Å for FC16 vs. ≈ 30 Å for WC14) is consistent with the different molecular structures. For FC16/ β ME, on the other hand, no significant differences in d_{SE} were observed for immersion times > 4 h (Fig. 1), suggesting that prolonged immersion does not increase molecular order further.

Figure 2 shows the FT-IRRAS features of pure FC16 SAMs in the C-H stretch region from 3500 cm^{-1} to 2500 cm^{-1} and the midrange from 1500 cm^{-1} to 750 cm^{-1} . The prominent band at 1132 cm^{-1} , assigned as the C-O and C-C stretching bands, and irregular baseline in the midrange region indicate a disordered nona(ethylene oxide) [NEO] segment³² that should be able to incorporate water in the presence of an aqueous environment. Absent in this region are any spectral features of helical³³ or all-trans³⁴ conformational order in the EO segment. The IR data suggests no order over any significant segment of the NEO chain. The C-H region is also largely featureless due to the overlap of the methylene stretching bands of the NEO segment and the methyl and methylene stretching bands of the hexadecyl chains. Discernible bands at 2966 cm^{-1} , 2917 cm^{-1} , and 2879 cm^{-1} are assigned as the ν_a (ip) (CH_3), ν_{as} (CH_2) and ν_s (FR) (CH_3) modes, respectively.³⁵ The absorption band at 2917 cm^{-1} suggests order in the alkyl chains, which is consistent with the earlier FT-IRRAS data on WC14 and the increased SE thickness data.

Sparsely-tethered bilayer lipid membranes: Zwitterionic lipids. Bilayers were formed from the precursor SAMs by rapid solvent exchange.¹⁰ We studied stBLMs completed with DPhyPC extensively in EIS measurements to compare the capability of FC16 to serve as the

basis for fluid, tightly-sealing membranes with that of WC14. DPhyPC-containing stBLMs at FC16:βME = 30:70 and 15:85 were structurally characterized with NR. Because success in the formation of WC14-based stBLMs containing anionic phospholipids has been variable in our hands, we also investigated a set of FC16-based samples formed from zwitterionic/anionic lipid mixtures.

Electrochemical Impedance spectroscopy. Figure 3A shows a series of EI spectra of FC16-based stBLMs with different FC16:βME from 100:0 to 10:90, completed with DPhyPC. The Cole-Cole plots show a systematic progression from spectra that consist of semicircles with small radii (corresponding to bilayer capacitances of $\approx 0.6 \mu\text{F}/\text{cm}^2$ for 100 mol% to 50 mol% of FC16) to subsequently larger semicircles (larger capacitances) that show low-frequency tails of increasing lengths. In earlier work⁹ we argued that the length of the tail is associated with the defect density of the stBLMs.

The inset in Fig. 3A shows the equivalent circuit model (ECM) used to determine the electrical characteristics of the stBLMs quantitatively. It uses constant-phase elements (CPEs) with an impedance defined as

$$Z_{CPE} = \frac{1}{CPE(i\omega)^\alpha} \quad (2)$$

to account for imperfections of the membrane, such as surface roughness with an empirically determined dependence on cyclic frequency, ω . As $\alpha \rightarrow 1$, this impedance is that of the capacitance of an ideal membrane, C_{membrane} . The CPE in the defect branch originates from in-plane components of the electric field surrounding a defect. This in-plane component decays with distance from the defect center and couples to the Helmholtz capacitance of the interface between the Au electrode and the submembrane space. The components in the grayed area of the ECM account for the conductivity of the bulk electrolyte and stray capacitances associated with the sample cell and cables.

In fitting the data with the ECM, Fig. 3A, we noticed that the resistance of the defect branch at high FC16 ratios was so large that it could not be reliably determined (note that the low-

frequency tails in the Cole-Cole plots that are well-developed for samples with high backfiller concentrations vanish for FC16: β ME > 50:50). The parameters that describe the defect branch are then ill-defined. Our approach was to fix α_{defect} at 0.5, which yielded R_{defect} values in the 3 M Ω cm² range, to determine CPE_{stBLM} . Foregoing the defect branch in the ECM altogether yielded very similar results for CPE_{stBLM} and α_{stBLM} . Figure 3B shows the development of the CPE amplitude and defect resistance R_{defect} as a function of anchor:backfiller composition, in which FC16-based stBLMs are compared with WC14-based stBLMs. Again consistent with expectations based on the differences in molecular structures between the two anchor molecules, FC16-based bilayers tend to have larger resistances and lower capacitances ($C \approx |CPE|$, since $\alpha \approx 1$). Table 2 shows the fit results in detail.

Neutron reflection. The backfiller concentration range we are most interested in is at large proportions of β ME where anchoring points of the membrane are well diluted and their interference with in-plane bilayer dynamics can be expected to be minimized. In the earlier studies of WC14, we observed that structurally well-defined and functionally intact, tightly sealed membranes were obtained for WC14: β ME ratios down to $\approx$ 30:70. All results discussed so far indicated that the FC16: β ME form well-defined membranes at even lower anchor densities. We therefore characterized FC16: β ME-based stBLMs with NR at 30:70 and at 15:85, in order to obtain a direct comparison with WC14 and to provide a reference system for the utilization of FC16 at even lower concentration in future work.

Figure 4A shows representative NR results for an stBLM of FC16: β ME = 30:70. Data have been normalized by the Fresnel reflectivity, R_F . The bilayer was completed with DPhyPC in D₂O and the NR spectrum measured. The buffer phase was then exchanged *in situ* for a H₂O/D₂O mixture with a neutron scattering length density (nSLD) $\rho_n = 4 \times 10^{-6}$ Å⁻² (“CM4”) and the NR measured and finally, the buffer phase was again exchanged for H₂O and the NR determined. A simultaneous fit to all three data sets was performed with a slab model that included 3 layers for the surface of the inorganic substrate (1: SiO_x, 2: Cr, 3: Au) and 4 layers for the stBLM structure (4: thiol/ β ME/hydrated tether/inner lipid headgroups, 5: inner alkane layer, 6: outer alkane layer, 7: outer phospholipid headgroups). The results, and those from a similar

set of measurements on an stBLM with FC16:βME = 15:85 (data not shown), are summarized in Table 3, and the corresponding nSLD profiles shown in Fig. 4B and 4C. The table shows also results for stBLMs completed with mixtures of zwitterionic and anionic phospholipids, POPC and POPG (see below).

The fact that all neutron data sets determined for isotopically contrasted samples can be well described by nSLD profiles derived from one unique model indicate that these stBLMs form laterally homogeneous bilayer structures. A close inspection of Fig. 4 shows that the profiles are consistent with structures in which the membrane is decoupled from the inorganic substrate by a nanometer-thin hydration layer. The solvent contents of the 4 distinct organic layers in each stBLM can be directly assessed from the model due to their characteristic differences in nSLD as a function of isotopic composition of the aqueous phases. This analysis shows that the water content in the ≈ 20 Å thick submembrane layer is on the order of 50 vol%. The alkane layers that form the hydrophobic cores of the membrane are essentially water-free. In the stBLMs formed on FC16:βME = 30:70, the monolayer proximal to the substrate is essentially free of solvent ($4\% \pm 3\%$). At 15:85, this monolayer contains some solvent, indicating that the inner leaflet is no longer completely reconstituted with phospholipid in the rapid solvent exchange at this higher dilution of the membrane anchor. The distal monolayer leaflets are defect free and show no indication of solvent inclusion in any of the samples. The PC headgroups are clearly recognized as regions of elevated nSLD at distances of ≈ 50 Å from the Au film in the profiles measured with H₂O solvent. In earlier NR measurements of Langmuir monolayers composed of DPPC, we determined the nSLD of the PC headgroup, $\rho_n^{PC} = 1.8 \times 10^{-6} \text{ Å}^{-2}$.³¹ In order to reduce the number of model parameters, we fixed their thickness generally at $d = 7$ Å, its approximate value,³¹ and constrained the nSLD of the slab such that the headgroups appeared well hydrated in the model (50 vol% water content). This value is close to the values typically observed for stBLMs based upon WC14 membrane anchors.¹⁰ Figure 5 shows parameter distributions (tether layer thicknesses and hydrophobic chain monolayer thicknesses for stBLMs of the two distinct SAM compositions, Fig. 5A) determined by MC resampling of the data that indicate that the extension of the teth-

ers and the hydrophobic membrane slab thickness both shrink as the lateral tether density is reduced. Not only are the NR measurements precise enough to measure these differences but the MC resampling also shows that these differences are indeed significant.

Sparsely-tethered bilayer lipid membranes: Zwitterionic/anionic lipid mixtures. We also investigated stBLMs formed on SAMs of FC16:βME = 30:70 using charged phospholipids. In earlier work with WC14, attempts to complete bilayers entirely with anionic phospholipids failed in that the resulting bilayers were often incomplete, and stBLMs formed from anionic/zwitterionic mixtures were also defect-rich with substantial water content in the hydrophobic membrane slabs (Heinrich & McGillivray, unpublished results). Here we tested mixtures of POPC and POPG (80:20) for their capacity to form structurally well-defined stBLMs on the basis of FC16 membrane tethers. Because it is likely that the relative amounts of POPC and POPG in the stBLM differ from that in the solution used to complete the bilayer and it is difficult to determine the stoichiometry of the lipids at the surface experimentally, we investigated two samples of different isotopic compositions. One sample was composed of hydrogenated phospholipids entirely while the second sample incorporated hydrogenated POPC and POPG on which the palmitoyl chain was perdeuterated (d_{31} -POPG).

Structural analysis (neutron reflection). The NR data (not shown) were modeled in a similar approach as that described for DPhyPC stBLMs and yielded nSLD profiles that were consistent with the formation of well-defined and laterally homogeneous and complete bilayer structures (Fig. 6A, B). A comparison of the fully hydrogenated and the partially deuterated sample shows that the preparation is reasonably reproducible in its geometric structure. Model parameters are also summarized in Table 3 for comparison with those of the zwitterionic stBLMs. As realized from the nSLD profiles and borne out in the table, the bilayers are indeed 100% complete and generally similar to the stBLMs completed with DPhyPC. Remarkably however, the thickness of the tether slab is marginally, but significantly, smaller than that observed with the zwitterionic phospholipid at the same FC16:βME = 30:70. Accordingly, the hydration of the submembrane space is somewhat lower in the charged samples than that for the zwitterionic lipids (Fig. 5B), possibly due to attraction of the charged headgroups to the

interface by image charges. Also, we observe a slightly reduced thickness of the hydrophobic membrane slabs, which reflects the higher intrinsic disorder of the unsaturated chains in comparison with the phytanoyl chains.

Combining the NR results for the fully hydrogenated sample with that for the sample in which POPG was deuterated on the *sn*-1 chain (Table 3, columns 3 and 4, respectively) allows an estimate of the proportions of PC and PG in the stBLM by virtue of the increase in nSLD in the distal lipid chain leaflet. Using the result for the fully hydrogenated sample, $\rho_n^{\text{chain}} = -0.31 \times 10^{-6} \text{ \AA}^{-2}$, we calculate an average area per lipid of the POPC/POPG mixture of $A = 68 \pm 7 \text{ \AA}^2$. In the sample formed with *d*-POPG, the proximal leaflet is devoid of deuterated label, indicating that the charged lipid remains entirely in the distal monolayer. From the observed nSLD of this layer, we estimate that the proportion of *d*-POPG in the mixture is $20\% \pm 5\%$.

Parameter confidence limits and parameter coupling. Given the general structure of the data, in which the pattern of interference minima appears strongly dominated by the structural features of the high-index Au film, it is particularly interesting to determine to what extent the structural parameters of the (mostly) low-index organic film features depend on the parameters of the Au film. The MC resampling procedure is also useful to assess correlations between the model parameters. Table 4 shows the covariance matrices for both POPC:POPG data sets. Correlations reflect directly the width of the parameter distributions, and therefore the size of the confidence interval given in Table 3, as illustrated in Fig. 7. The analysis reveals strong correlations between the layer properties of the SiO_x, Cr, and Au films. Correlations between the Au film and the organic overlayers are not nearly as strong. Particularly the correlations between the Au and Cr film structure (Fig. 7A) suggest inadequacies of the model for the chemically complex Cr bonding layer and indicate interdiffusion of Au atoms into the Cr layer resulting in a nSLD much larger than that for pure Cr (and/or a larger roughness of the Cr/Au interface). We chose to model the Cr layer with an nSLD that is substantially higher than that expected for pure Cr ($\rho_n^{\text{Cr}} \approx 3 \times 10^{-6} \text{ \AA}^{-2}$) and use a roughness parameter, σ , identical to the roughness of all other interfaces (global roughness approach).

Strong correlations are also observed between the proximal lipid leaflet and the tether layer (Fig. 7B), possibly deriving from an oversimplification in modeling the chemically complex tether region whereas correlation between the Au film and the organic layers is weak (Fig. 7C, D). There is no evidence that ‘domination’ of the NR spectrum by the Au film impairs the determination of the structure of the stBLM. In both cases where correlations are high, those occur in a very narrow (confidence) interval, so that the affected parameters can still be determined with high precision. For example, substrate layer thicknesses are typically determined from the NR data to ± 3 Å, and thicknesses of layers in the stratified organic surface architecture ± 1 Å. A probability plot for the nSLD profiles of the 80:20 mol:mol POPC:*d*-POPG stBLM in D₂O derived from the MC resampling (Fig. 8) illustrates this point impressively. This depiction visualizes the implications of parameter coupling and shows that the main range of uncertainty in the nSLD profiles is located at the Cr/Au interface and that those uncertainties do not transcend into the organic surface architecture, as is realized by the observation of a sharp interface between the Au film and the tether layer.

IV. DISCUSSION

Similar to WC14-anchored bilayers, FC16-based stBLMs are highly insulating on SAMs without β ME, or at low backfiller concentrations. However, tBLMs without backfiller do not contain solvent in the submembrane layer, typically < 5 vol%,¹⁰ and are not particularly well suited for membrane protein incorporation (McGillivray et al., unpublished). Backfilling results in the lateral dilution of membrane anchors and renders the stBLM amenable to the reconstitution of proteins, such as α -hemolysin (α HL).¹³ As shown earlier, there is a limit to dilution of the membrane anchor in the SAMs at which its hydrophobic chains do not attain an upright orientation on the Au surface. While rapid solvent exchange may still lead to the formation of well-ordered bilayer structures, such stBLMs show progressively poorer electrical resistances with increasing proportions of β ME. We reasoned that an extension of the polymethylene chains on the membrane anchor might promote the formation of stBLMs in which the anchor density could be further reduced. Importantly, the increased tether length may increase the thickness

of the submembrane space and the flexibility of the anchored lipid thereby potentially offsetting reductions in membrane fluidity that might arise from the increase in dispersion interactions.

All results presented here bear out these expectations, although the differences between FC16-based and WC14-based stBLMs, particularly in their electrical parameters, are rather moderate. Nevertheless, all structural and functional metrics indicate that stBLMs are well-organized at lower tether densities with FC16 than with WC14. Moreover, as judged from our initial attempt, mixed membranes containing anionic phospholipids form more readily on FC16-based SAMs than on WC14.

In structural terms, the bilayers formed on FC16 are extremely well-defined. Down to FC16:βME = 25:75, bilayers are virtually defect-free by NR and EIS data. Only at FC16:βME = 15:85 does NR start to show water-filled defects in the hydrophobic bilayer core by virtue of isotopic contrast variation of the aqueous buffer. The thickness of the submembrane space is slightly larger with FC16 than with WC14 (≈ 20 Å vs. ≈ 15 Å). As with WC14, it is thinner than the extended length of the oligo(ethylene oxide) spacer, consistent with the IR results indicating disordered oligo(ethylene oxide) chains. The submembrane layer is highly hydrated, particularly at high dilution of the membrane anchor ($\geq 50\%$ of water by volume).

As estimated from the observed nSLD of the hydrophobic membrane interior, the lateral area per phospholipid within the bilayers is $A \approx 70$ Å² (POPC/POPG), a value which is comparable with that reported for fully hydrated POPC multibilayer membranes,³⁶ and $A \approx 75$ Å² (DPhyPC) which is slightly less than the value estimated from x-ray scattering.³⁷ From these results one would expect that the mobility of phospholipids in the stBLMs should be comparable to that in free lipid bilayers – at least in the monolayer leaflet distal with respect to the inorganic substrate. Diffusion measurements using fluorescence correlation spectroscopy (FCS) of labeled phospholipids in such stBLMs indicate that the mobility is indeed somewhat reduced but of the same order of magnitude (Moldovan, Shenoy & Lösche, preliminary results).

The notion that the proximal and distal monolayer sheets may be distinctly different in the stBLMs is borne out in the NR experiments with palmitoyl-perdeuterated POPG. The results indicate that d-POPG partitions entirely into the distal monolayer where the PC:PG ratio is approximately the same as in the immersion solution used for the rapid solvent exchange. In fact, the apparent nSLD drop of the proximal chain monolayer from the value observed in fully hydrogenated phospholipid (POPC/POPG) to that of the hydrogenated/deuterated mixture (POPC/d-POPG) suggests that the deuterated compound is quantitatively excluded from the proximal leaflet. One might have expected that the nominal nSLD values of the membrane interior in the POPC/POPG stBLM and of the proximal leaflet in the POPC/d-POPG stBLM should be identical. However, even while the precision of the nSLD value in the latter case is reduced, we note that there may be, in fact, differences in the average densities of the proximal and distal layers due to the distinct chain ligations in phospholipids (acyl chains) and in the membrane anchor (alkyl chains). Because the alkyl chains can pack more densely, the proximal layer may be of a higher density than the distal layer. For fully hydrogenated lipids we cannot discriminate in the NR model between those monolayers, the nSLD values observed there may represent an average between two different densities.

In the limited range of lipids that we have so far used to form stBLMs based upon FC16, we observed consistently that the submembrane space in partially charged bilayers is slightly reduced from the values observed for fully zwitterionic bilayers. This leads us to the interesting hypothesis, to be tested in future work, that electrostatic forces increase the attraction of charged headgroups to the conducting Au film and lead to a reduction in equilibrium distance of the bilayer from the surface.

V. CONCLUSIONS

We investigated and compared quantitatively the structural and functional properties of stBLMs based upon two different membrane lipid anchors backfilled with β ME. FC16, which comprises longer polymethylene chains (dipalmityl) and hydrophilic oligo(ethylene oxide) tether (9 ethylene oxide units) than WC14 (dimyristyl and 6 ethylene oxide units), forms bilay-

ers that show increased resistivity to ion transfer. The submembrane space is by ≈ 0.5 nm wider for FC16-based stBLMs than for WC14-based stBLMs. stBLMs that include charged phospholipids comprise well-defined, complete bilayers with FC16/ β ME. The charged component, DOPG, incorporates into the outer monolayer leaflet in the same ratio as provided in the immersion solution, but is excluded from the inner leaflet. In all cases we investigated here, the area densities of the lipids within the bilayers were on average close to those in free bilayer membranes. Particularly for charged phospholipids, FC16 provides a distinct advantage over WC14 for the formation of well-defined stBLMs.

ACKNOWLEDGMENTS

Support by the National Institute of Standards and Technology (U.S. DOC) in providing the neutron research facilities used in this work is gratefully acknowledged. T. Ng was supported by the SURF program funded in part by the NSF (DMR-0454672). This work was further supported by the NSF (CBET-0555201) and the American Health Assistance Foundation (A2008-307).

REFERENCES

1. Rietveld, A.; Simons, K., The differential miscibility of lipids as the basis for the formation of functional lipid rafts. *Biochim. Biophys. Acta* **1998**, 1376, 467-479.
2. Singer, S. J.; Nicolson, G. L., The fluid mosaic model of the structure of cell membranes. *Science* **1972**, 173, 720-731.
3. Brian, A. A.; McConnell, H. M., Allogenic stimulation of cytotoxic T cells by supported planar membranes. *Proc. Natl. Acad. Sci. USA* **1984**, 81, 6159-6163.
4. Tamm, L. K.; McConnell, H. M., Supported phospholipid bilayers. *Biophys. J.* **1985**, 47, 105-113.
5. Cornell, B. A.; Braach-Maksvytis, V. L. B.; King, L. B.; Osman, P. D. J.; Raguse, B.; Wieczorek, L.; Pace, R. J., A biosensor that uses ion-channel switches. *Nature* **1997**, 387, 580-583.
6. Sackmann, E., Supported membranes - Scientific and practical applications. *Science* **1996**, 271, 43-48.
7. Stora, T.; Lakey, J. H.; Vogel, H., Ion-channel gating in transmembrane receptor proteins: Functional activity in tethered lipid membranes. *Angew. Chem. Int. Ed. Engl.* **1999**, 38, 389-392.
8. Knoll, W.; Frank, C. W.; Heibel, C.; Naumann, R.; Offenhäuser, A.; Rühle, J.; Schmidt, E. K.; Shen, W. W.; Sinner, A., Functional tethered lipid bilayers. *Rev. Mol. Biotechn.* **2000**, 74, 137-158.
9. Tanaka, M.; Sackmann, E., Polymer-supported membranes as models of the cell surface. *Nature* **2005**, 437, 656-663.
10. McGillivray, D. J.; Valincius, G.; Vanderah, D. J.; Febo-Ayala, W.; Woodward, J. T.; Heinrich, F.; Kasianowicz, J. J.; Lösche, M., Molecular-scale structural and functional characterization of sparsely tethered bilayer lipid membranes. *Biointerphases* **2007**, 2, 21-33.
11. Valincius, G.; McGillivray, D. J.; Febo-Ayala, W.; Vanderah, D. J.; Kasianowicz, J. J.; Lösche, M., Enzyme activity to augment the characterization of tethered bilayer membranes. *J. Phys. Chem. B* **2006**, 110, 10213-10216.
12. Valincius, G.; Heinrich, F.; Budvyte, R.; Vanderah, D. J.; McGillivray, D. J.; Sokolov, Y.; Hall, J. E.; Lösche, M., Soluble amyloid β -oligomers affect dielectric membrane properties by bilayer insertion and domain formation: Implications for cell toxicity. *Biophys. J.* **2008**, 95, 4845-4861.
13. McGillivray, D. J.; Valincius, G.; Heinrich, F.; Robertson, J. W. F.; Vanderah, D. J.; Febo-Ayala, W.; Ignatjev, I.; Lösche, M.; Kasianowicz, J. J., Functional reconstitution of *Staphylococcus aureus* α -hemolysin in tethered bilayer lipid membranes. *Biophys. J.* **2008**, in press.

14. Raguse, B.; Braach-Maksvytis, V. L. B.; Cornell, B. A.; King, L. B.; Osman, P. D. J.; Pace, R. J.; Wieczorek, L., Tethered lipid bilayer membranes: Formation and ionic reservoir characterization. *Langmuir* **1998**, 14, 648-659.
15. Vockenroth, I. K.; Ohm, C.; Robertson, J. W. F.; McGillivray, D. J.; Lösche, M.; Köper, I., Stable insulating tethered bilayer membranes. *Biointerphases* **2008**, 3, FA68 - FA73.
16. Holt, S. A.; Le Brun, A. P.; Majkrzak, C. F.; McGillivray, D. J.; Heinrich, F.; Lösche, M.; Lakey, J. H., An ion channel containing model membrane: Structural determination by magnetic contrast neutron reflectometry. *Soft Matter* **2008**, submitted.
17. Kent, M. S.; Yim, H.; Murton, J. K.; Satija, S.; Majewski, J.; Kuzmenko, I., Oligomerization of membrane-bound diphtheria toxin (CRM197) facilitates a transition to the open form and deep insertion. *Biophys. J.* **2008**, 94, 2115-2127.
18. Wymann, M. P.; Schneiter, R., Lipid signalling in disease. *Nat. Rev. Mol. Cell Bio.* **2008**, 9, 162-176.
19. Liu, B.; Zhou, Z., Lamin A/C, laminopathies and premature ageing. *Histol. Histopathol.* **2008**, 23, 747-63.
20. Certain commercial materials, equipment, and instruments are identified in this manuscript in order to specify the experimental procedure as completely as possible. In no case does such identification imply a recommendation or endorsement by the National Institute of Standards and Technology, nor does it imply that the materials, equipment, or instruments identified are necessarily the best available for the purpose.
21. Vanderah, D. J.; Valincius, G.; Meuse, C. W., Self-assembled monolayers of methyl 1-thiahexa(ethylene oxide) for the inhibition of protein adsorption. *Langmuir* **2002**, 18, 4674-4680.
22. Vanderah, D. J.; Arsenault, J.; La, H.; Gates, R. S.; Silin, V.; Meuse, C. W.; Valincius, G., Structural variations and ordering conditions for the self-assembled monolayers of HS(CH₂CH₂O)₍₃₋₆₎CH₃. *Langmuir* **2003**, 19, 3752-3756.
23. Vanderah, D. J.; Gates, R. S.; Silin, V.; Zeiger, D. N.; Woodward, J. T.; Meuse, C. W.; Valincius, G.; Nickel, B., Isostructural self-assembled monolayers. 1. Octadecyl 1-thia-oligo(ethylene oxides). *Langmuir* **2003**, 19, 2612-2620.
24. Trasatti, S.; Petrii, O. A., Real surface area measurements in electrochemistry. *Pure Appl. Chem.* **1991**, 63, 711-734.
25. Lu, J. R.; Thomas, R. K.; Penfold, J., Surfactant layers at the air/water interface: Structure and composition. *Adv. Colloid Interf. Sci* **2000**, 84, 143-304.
26. Vacklin, H. P.; Tiberg, F.; Fragneto, G.; Thomas, R. K., Composition of supported model membranes determined by neutron reflection. *Langmuir* **2005**, 21, 2827-2837.
27. Dura, J. A.; Pierce, D.; Majkrzak, C. F.; Maliszewskyj, N.; McGillivray, D. J.; Lösche, M.; O'Donovan, K. V.; Mihailescu, M.; Perez-Salas, U. A.; Worcester, D. L.; White, S. H.,

- AND/R: A neutron diffractometer/reflectometer for investigation of thin films and multilayers for the life sciences. *Rev. Sci. Instrum.* **2006**, 77, 074301.
28. Kienzle, P. A.; Doucet, M.; McGillivray, D. J.; O'Donovan, K. V.; Berk, N. F.; Majkrzak, C. F. *ga_refl*, 2000-2006.
 29. Parratt, L. G., Surface studies of solids by total reflection of x-rays. *Phys. Rev.* **1954**, 95, 359-369.
 30. Press, W. H.; Flannery, B. P.; Teukolsky, S. A.; Vetterling, W. T., *Numerical Recipes*. Cambridge University Press: Cambridge, 1986.
 31. Vaknin, D.; Kjaer, K.; Als-Nielsen, J.; Lösche, M., Structural properties of phosphatidylcholine in a monolayer at the air/water interface. Neutron reflection study and reexamination of x-ray reflection experiments. *Biophys. J.* **1991**, 59, 1325-1332.
 32. Dissanayake, M. A. K.; Frech, R., Infrared spectroscopic study of the phases and phase transitions in poly(ethylene oxide) and poly(ethylene oxide)-lithium trifluoromethanesulfonate complexes. *Macromolecules* **1995**, 28, 5312-5319.
 33. Vanderah, D. J.; Meuse, C. W.; Silin, V.; Plant, A. L., Synthesis and characterization of self-assembled monolayers of alkylated 1-thiahexa(ethylene oxide) compounds on gold. *Langmuir* **1998**, 14, 6916-6923.
 34. Harder, P.; Grunze, M.; Dahint, R.; Whitesides, G. M.; Laibinis, P. E., Molecular conformation in oligo(ethylene glycol)-terminated self-assembled monolayers on gold and silver surfaces determines their ability to resist protein adsorption. *J. Phys. Chem. B* **1998**, 102, 426-436.
 35. Hussain, H.; Kerth, A.; Blume, A.; Kressler, J., Amphiphilic block copolymers of poly(ethylene oxide) and poly(perfluorohexylethyl methacrylate) at the water surface and their penetration into the lipid monolayer. *J. Phys. Chem. B* **2004**, 108, 9962-9969.
 36. Kucerka, N.; Liu, Y. F.; Chu, N.; Petrache, H. I.; Tristram-Nagle, S.; Nagle, J. F., Structure of fully hydrated fluid phase DMPC and DLPC lipid bilayers using X-ray scattering from oriented multilamellar arrays and from unilamellar vesicles. *Biophys J* **2005**, 88, 2626-2637.
 37. Wu, Y.; He, K.; Ludtke, S. J.; Huang, H. W., X-ray diffraction study of lipid bilayer membranes interacting with amphiphilic helical peptides: Diphytanoyl phosphatidylcholine with alamethicin at low concentrations. *Biophys. J.* **1995**, 68, 2361-2369.

TABLES

Table 1: Ellipsometric thicknesses, d_{SE} , and contact angles, θ , of FC16/ β ME SAMs as a function of FC16: β ME mol% ratio in the adsorption solutions. Uncertainties of d_{SE} reflect variabilities of measurements across one wafer. The ellipsometric thicknesses of different preparations (wafers) may vary more than the quoted uncertainties. Uncertainties of θ are standard deviations of typically four measurements per sample.

fraction of FC16 / mol%	ellipsometric thickness / Å (4 h immersion)	contact angle / °
0	3.5 ± 0.3	33 ± 5
10	13.0 ± 0.2	75 ± 3
20	16.8 ± 0.4	82 ± 3
30	20.6 ± 0.3	82 ± 3
40	21.9 ± 0.4	87 ± 3
50	41.9 ± 0.4	106 ± 2
60	42.7 ± 0.4	106 ± 1
70	44.7 ± 0.4	106 ± 2
80	43.1 ± 0.4	106 ± 1
90	43.6 ± 0.4	107 ± 2
100	43.1 ± 0.4	109 ± 1

Table 2: Best-fit parameters for EI spectra of stBLMs completed with DPhyPC. Varying FC16:βME from 100:0 to 10:90 were used for the preparation of the parent SAM in the immersion solution. Averages were derived from at least 3 independent samples.

fraction of FC16 / mol%	100	75	50	40	35	30	25	20	15	10
$CPE_{\text{stBLM}} / \mu\text{Fcm}^{-2}\text{s}^{(\alpha-1)}$	0.62 ± 0.03	0.63 ± 0.01	0.65 ± 0.02	0.74 ± 0.06	0.80 ± 0.04	0.85 ± 0.01	0.75 ± 0.02	0.92 ± 0.02	0.85 ± 0.06	1.09 ± 0.12
α_{stBLM}	0.997 ± 0.001	0.998 ± 0.001	0.996 ± 0.001	0.991 ± 0.003	0.994 ± 0.003	0.991 ± 0.005	0.995 ± 0.002	0.989 ± 0.002	0.991 ± 0.003	0.972 ± 0.015
$CPE_{\text{defect}} / \mu\text{Fcm}^{-2}\text{s}^{(\alpha-1)}$	n/a	n/a	0.92 ± 0.42	4.22 ± 1.77	1.07 ± 0.29	3.81 ± 0.59	2.48 ± 1.10	8.54 ± 0.96	4.65 ± 0.80	10.1 ± 1.2
α_{defect}	n/a	n/a	0.521 ± 0.077	0.442 ± 0.059	0.501 ± 0.057	0.459 ± 0.105	0.417 ± 0.039	0.601 ± 0.111	0.382 ± 0.096	0.741 ± 0.033
$R_{\text{defect}} / \text{k}\Omega\text{cm}^2$	> 1000	> 1000	731 ± 402	631 ± 246	299 ± 103	117 ± 70	180 ± 98	33.4 ± 12.9	40.0 ± 9.4	10.9 ± 4.7
fit quality / 10 ⁻⁵	1.84	1.16	1.52	2.23	2.91	3.52	1.83	3.22	1.23	6.25

Table 3: Best-fit NR models of the investigated stBLMs.

parameter	FC16:βME = 30:70; DPhyPC	FC16:βME = 15:85; DPhyPC	FC16:βME = 30:70; POPC:POPG = 80:20	FC16:βME = 30:70; <i>h</i> -POPC: <i>d</i> -POPG = 80:20
layer thicknesses / Å				
<i>d</i> _{SiO_x}	27.6 ± 1.1	27.5 ± 1.4	29.9 ± 1.8	37.3 ± 1.6
<i>d</i> _{Cr}	25.8 ± 1.9	25.8 ± 2.3	23.6 ± 2.5	13.6 ± 3.1
<i>d</i> _{Au}	116.9 ± 1.7	116.5 ± 2.6	124.4 ± 1.7	122.6 ± 2.1
<i>d</i> _{tether}	21.1 ± 0.7	18.3 ± 0.9	15.4 ± 0.7	17.2 ± 1.4
<i>d</i> _{lipid chains}	15.5 ± 0.3	14.9 ± 0.4	12.7 ± 0.4	13.2 ± 0.7
<i>d</i> _{outer lipid headgroup}	7 (fixed)			
neutron scattering length densities / 10 ^{−6} Å ^{−2}				
<i>ρ_n</i> ^{SiO_x}	3.50 ± 0.05	3.49 ± 0.06	3.4 (fixed)	3.4 (fixed)
<i>ρ_n</i> ^{Cr}	4.22 ± 0.04	4.19 ± 0.05	4.0 (fixed)	4.0 (fixed)
<i>ρ_n</i> ^{Au}	4.44 ± 0.02	4.40 ± 0.02	4.40 ± 0.01	4.37 ± 0.01
<i>ρ_n</i> ^{tether}	1.07 ± 0.17	1.15 ± 0.19	1.0 (fixed)	1.0 (fixed)
<i>ρ_n</i> ^{inner lipid chains}	−0.36 ± 0.05	−0.38 ± 0.06	−0.31 ± 0.05	−0.49 ± 0.15
<i>ρ_n</i> ^{outer lipid chains}				+0.60 ± 0.10
<i>ρ_n</i> ^{outer lipid headgroup}	1.79 (fixed)			
volume fractions of layer content				
water <i>vf</i> _{tether}	0.53 ± 0.02	0.49 ± 0.03	0.18 ± 0.03	0.23 ± 0.03
alkane <i>vf</i> _{inner lipid ch}	0.96 ± 0.03	0.91 ± 0.04	1.00 ± 0.01	1.00 ± 0.01
alkane <i>vf</i> _{outer lipid ch}	1.00 ± 0.01	1.00 ± 0.03	1.00 ± 0.01	1.00 ± 0.01
water <i>vf</i> _{outer lipid hg}	0.50 (fixed)			
roughness / Å				
σ	5.8 ± 0.6	5.8 ± 1.0	5.0 ± 0.9	5.0 ± 0.2
χ ²	3.32	2.74	2.33	2.86

Table 4: Covariance matrices of the best-fit model parameters for the NR data sets from FC16-based (FC16:βME = 30:70) stBLMs completed with 80:20 POPC:d-POPC (lower left triangle) and 80:20 h-POPC:h-POPG (upper right triangle).

	d_{SiO_x}	d_{Cr}	d_{Au}	d_{tether}	$d_{\text{lipid chains}}$	vf_{tether}	$vf_{\text{inner lipid ch}}$	$vf_{\text{outer lipid ch}}$	ρ_n^{Au}	$\rho_n^{\text{inner lipid ch}}$	$\rho_n^{\text{outer lipid ch}}$	$\rho_n^{\text{D}_2\text{O}}$	ρ_n^{CM4}	σ
d_{SiO_x}		-0.72	0.20	-0.25	0.15	0.17	0.04	-0.05	0.21	0.20		-0.03	-0.04	-0.21
d_{Cr}	-0.86		-0.80	0.19	-0.05	-0.19	0.00	0.01	0.12	-0.11		0.02	0.01	0.16
d_{Au}	0.64	-0.93		-0.10	-0.08	0.20	-0.02	0.01	-0.36	-0.02		-0.01	0.02	-0.01
d_{tether}	-0.09	0.15	-0.23		-0.84	0.26	0.05	0.06	-0.11	-0.74		-0.05	-0.01	0.23
$d_{\text{lipid chains}}$	0.02	-0.06	0.09	-0.93		-0.65	-0.05	-0.07	0.17	0.84		0.09	0.08	-0.39
vf_{tether}	0.20	-0.20	0.20	0.54	-0.77		0.01	0.01	-0.06	-0.36		-0.18	-0.11	0.25
$vf_{\text{inner lipid ch}}$	-0.06	0.11	-0.14	0.33	-0.27	0.05		-0.05	0.02	-0.02		-0.01	-0.01	0.06
$vf_{\text{outer lipid ch}}$	0.00	-0.01	0.00	0.01	0.00	-0.03	0.05		-0.04	-0.07		0.01	-0.01	0.10
ρ_n^{Au}	0.02	0.18	-0.35	0.17	-0.04	-0.12	0.08	-0.04		0.26		0.24	-0.02	-0.08
$\rho_n^{\text{inner lipid ch}}$	0.16	-0.19	0.19	-0.81	0.80	-0.50	-0.10	-0.01	-0.07			0.12	0.01	-0.49
$\rho_n^{\text{outer lipid ch}}$	-0.14	0.18	-0.20	0.54	-0.43	0.24	0.31	0.02	0.20	-0.70				
$\rho_n^{\text{D}_2\text{O}}$	-0.05	0.08	-0.10	0.05	-0.02	-0.12	-0.08	-0.01	0.23	0.00	0.03		-0.04	-0.01
ρ_n^{CM4}	-0.06	0.03	0.01	-0.05	0.10	-0.14	0.00	0.10	-0.09	0.05	-0.07	-0.03		-0.02
σ	-0.01	-0.02	0.03	-0.06	0.07	-0.08	0.00	0.08	-0.03	0.01	-0.02	-0.03	0.03	

FIGURES

Scheme 1: Synthesis of FC16.

(a) 3 eq. NaH/THF, followed by 3 eq. C₁₆H₃₃Br, 42°C, 3d, 65%. (b) CH₃CO₂/THF/H₂O (4/2/1), 50°C, 7h, 68%. (c) NaH/THF, followed by Cl(CH₂CH₂O)₃THP, 45°C, 5d, 55%. (d) (C₆H₅)₃P then N-bromosuccinimide, CH₂Cl₂, 12 h, RT, 89%. (e) CH₃COS⁻Na⁺/CH₃OH, 7 h, 80%. (f) 1 N HCl/CH₃OH, reflux, 8 h, 90%.

Figure 1: Ellipsometric thickness of SAMs based upon FC16 or WC14 (data from ref. 10) as a function of tether spacing by increasing amount of β ME in the adsorption solution. Dashed lines are guides for the eye. Inset: Molecular structure of the two membrane anchors.

Figure 2: Two independently measured FT-IRRA spectra of 100% FC16 SAMs

Figure 3: EIS data of stBLMs completed with DPhyPC, and derived electrical parameters. (A) The main panel and upper left inset shows Cole-Cole plots of FC16-based stBLMs. Seven data sets with βME backfiller ratios as indicated are plotted in the main panel, where the length of the low-frequency tails correlates with the defect density in the bilayer.¹⁰ In the inset, data sets for FC16:βME = 10:90 and 50:50 have been omitted for clarity. The ECM used to model the data is shown in the lower right. (B, C) Membrane CPE amplitudes (approx. equivalent to membrane capacitances) and defect resistivities of FC16-based stBLMs derived from data such as those shown in (A) by fitting to the ECM. Corresponding results for WC14-based stBLMs (data from ref. 10) could not be determined at comparably low tether densities as for FC16. Dashed lines are guides for the eye.

Figure 4: NR data and resulting nSLD profiles for FC16-based stBLMs completed with DPhyPC. (A, B) Data and nSLD profiles for FC16: β ME = 30:70. (C) nSLD profiles for FC16: β ME = 15:85. The neutron reflection data in panel (A) have been normalized by the reflectivity of the idealized Si/buffer interface, i.e., the Fresnel reflectivity R_F . This representation visualizes better the interference pattern, particularly at high momentum transfer.

Figure 5: Histograms of best-fit parameter values for layer thicknesses in the slab models that describe the NR data from FC16-based stBLMs.

Figure 6: Neutron scattering length density profiles for FC16-based stBLMs (FC16: β ME = 30:70) completed with POPC:POPG (80:20) in the solution used in the rapid solvent exchange. (A) Both phospholipid species hydrogenated. (B) POPC:d-POPG. The inorganic substrate is not shown in this view but is similar to the one shown in Fig. 4 B, C.

Figure 7: Exemplary visualization of parameter correlations (Table 4) in the modeling of NR spectra by Monte Carlo resampling of the data. For the FC16-based stBLM (FC16:βME = 30:70) completed with POPC:d-POPG (80:20) in the solution used for rapid solvent exchange, these plots show the distribution of parameter pairs in the best-fit models that describe resampled virtual data sets. (A) d_{Au} vs. d_{Cr} ; covariance coefficient, $\eta = -0.93$ (B) $d_{lipid\ chains}$ vs. d_{tether} ; $\eta = -0.93$ (C) d_{Au} vs. $d_{lipid\ chains}$; $\eta = 0.09$ (D) d_{Au} vs. d_{tether} ; $\eta = -0.23$

Figure 8: Result from the MC resampling of NR data. A probability plot (FC16:βME = 30:70 stBLM completed with POPC:d-POPG=80:20) shows a superposition of all nSLD profiles in which shades of gray visualize the frequency of by which a grid point is hit. Black codes for 100 or more of a total of 1000 occurrences. This view gives a visual impression of how well certain regions in the surface architecture are determined by the NR data sets.